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Short Communication

Electroanalysis Using Differential Pulse Methods at a Microelectrode

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Abstract

This communication characterises the differential pulse voltammetric response of ultramicroelectrodes in connection with two different models.

Keywords: Microelectrodes, Differential pulse voltammetry

Microelectrodes have been cited to have many advantages over conventional electrodes [1–3]. However, a primary disadvantage is that the use of a microelectrode in a potential sweep mode results in a sigmoidal output which is difficult to interpret at low analyte concentrations. The aim of this work is to characterize the differential current response of a microelectrode. This may be done by numerical differentiation of a digitally acquired signal following a linear sweep which is trivial [4], or through the use of an applied differential pulse waveform.

The following assumptions were made in postulating the theory for differential pulse voltammetry at a planar disk microelectrode [5] and are the basis for Model 1.

- The Cottrell equation may be used for characterization of the current response at short time periods following the pulse.
- The current due to the potential ramp follows the traditional microelectrode behavior with a potential dependent component.
- The above two currents, a) and b), are additive for an electrochemically reversible reduction, thus

$$i_1 = \frac{nFAC\sqrt{D}}{\sqrt{\pi\delta}} \left[\frac{1 - \sigma^2}{(1 + \epsilon_1)(1 + \sigma^2\epsilon_1)} \right] \quad (1)$$

where

$$\sigma^2 = \exp\left(\frac{nF\Delta E}{RT}\right) \quad (2)$$

$$i_2 = \frac{4nFrDC}{1 + \epsilon_1} \quad (3)$$

where

$$\epsilon_1 = \exp\left(\frac{nF(E_1 - E^0)}{RT}\right) \quad (4)$$

$$i_3 = \frac{4nFrDC}{1 + \epsilon_2} \quad (5)$$

where

$$\epsilon_2 = \exp\left(\frac{nF(E_2 - E^0)}{RT}\right) \quad (6)$$

Where i_1 is the current contribution from the pulse alone, i_2 is the current due to the potential ramp before the pulse is applied, taking the limiting steady-state current to be

$$i_L = 4nFrDC \quad (7)$$

where r is the electrode radius, n is the number of electrons involved, F is the Faraday constant and D and C are the diffusion

coefficient and the concentration of the electroactive species. i_3 is the current due to the potential ramp at a time $(\delta + \tau)$, if the pulse was not applied. E_1 is the potential prior to pulse (at a time τ), E_2 is the potential defined by the potential ramp if the pulse was not applied (at a time $\delta + \tau$). τ is the time at which the current is sampled before the pulse is applied and $(\delta + \tau)$ is the time at which the current is sampled after the pulse is applied. ΔE is the pulse amplitude and all other symbols have their usual meaning. The instrumental differential output is represented as follows by the sum of the current due to the underlying ramp at time $(\delta + \tau)$, i_3 , and the current due to the pulse i_1 , less the current before the pulse i_2 .

$$\delta i = i_1 + i_3 - i_2 \quad (8)$$

In practice during the timescale of the experiment the diffusion layer thickness was found to be of the same order of magnitude as the diameter of the microelectrode. This facilitated the presence of "edge effects" which leads to a steady-state current being reached within the pulse width (δ). By modifying the theory the differential current may be calculated as follows using Model 2.

$$\delta i^* = i_4 - i_2 \quad (9)$$

where

$$i_4 = \frac{4nFrDC}{1 + \epsilon_3} \quad (10)$$

and

$$\epsilon_3 = \exp\left(\frac{nF(E_2 + \Delta E - E^0)}{RT}\right) \quad (11)$$

where i_4 is the steady-state current following the pulse and i_2 is the current due to the ramp potential before the pulse is applied. This modified theory allows for steady-state current to occur before and after the pulse.

From the limiting current (i_L) of the voltammetric response obtained by scanning the potential of a platinum microelectrode in a solution of 5×10^{-3} M ferrocyanide in a solution of 0.1 M KCl, the electrode radius was found from Equation 7. Taking i_L to be 5.60×10^{-9} A, and the diffusion coefficient (D) for $[\text{Fe}(\text{CN})_6]^{4-}$ to be 6.5×10^{-6} cm²s⁻¹ [6] the electrode radius (r) was calculated as 4.46×10^{-6} m.

Figure 1 shows the response obtained by the application of a differential pulse waveform to a platinum microelectrode in a solution of 5 mM $[\text{Fe}(\text{CN})_6]^{4-}$. It can be seen that the peak current heights increase with increasing pulse amplitude but at the expense of return to baseline. Closer investigation revealed that the increase in peak current height was linear with pulse amplitude over a

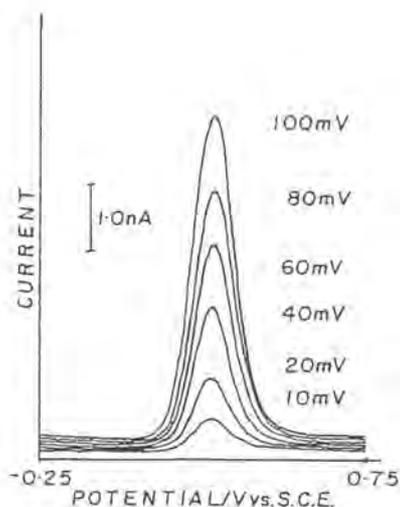


Fig. 1. Differential pulse output for a microelectrode in a solution of 5 mM $[\text{Fe}(\text{CN})_6]^{4-}$ in 0.1M KCl. Instrumental time constant: 1 s, sweep rate: 10 mV/s. Differential pulse waveform period: 1.0 s, pulse width: 55×10^{-3} s. Pulse amplitudes are shown in the figure.

limited range. The effect of varying the differential pulse waveform period (taken here to be the time between pulse applications) was also investigated. It was found that long differential pulse waveform periods (>1.0 s) resulted in stepped responses with ill-defined peaks while shorter differential pulse waveform periods resulted in smoother traces with well-defined peaks. The magnitude of the differential pulse waveform period was found to have negligible effect on peak current heights.

Figure 2 compares the experimental results obtained from the numerical derivative of a sigmoidal experimental plot, Figure 2a, and the response from the application of a differential pulse waveform to the same electrode, Figure 2b. Also included are simulated plots using Equation 8, Figure 2c, and Equation 9, Figure 2d. It is immediately obvious that Model 1 (Eq. 8), does not

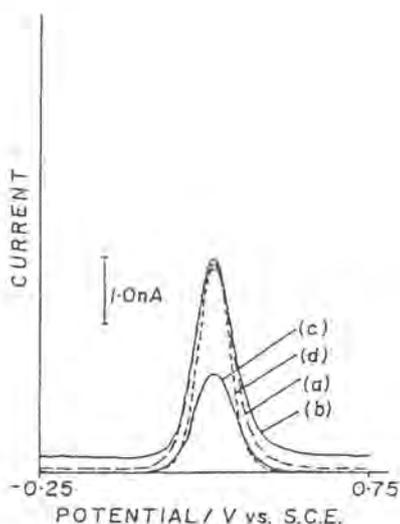


Fig. 2. a) Numerical point by point derivative of a linear sweep response for 5 mM $[\text{Fe}(\text{CN})_6]^{4-}$ in 0.1M KCl at a microelectrode ($r = 4.46 \times 10^{-6}$ m) where the sweep rate was 10 mV/s. Points which gave a pulse height of 60 mV were chosen. b) Experimental differential pulse output ($\Delta E = 60$ mV), sweep rate: 10 mV/s, time constant: 1 s. c) Model 1, (Eq. 8) calculated using the parameters as above. d) Model 2, (Eq. 9) calculated using the parameters as above.

Table 1. Comparison of the various theoretical models with the experimental data. Conditions as in Figure 2.

Pulse amplitude [mV]	Experimental differential pulse peak height [nA]	Peak heights from Model 1 [nA]	Peak heights from Model 2 [nA]	Numerical derivative peak heights [nA]
100	4.98	1.45	4.29	4.23
80	3.80	1.29	3.76	3.61
60	2.98	1.05	3.05	2.90
40	1.85	0.76	2.19	2.09
20	0.65	0.43	1.14	1.09

correlate well with either of the experimental traces whereas Model 2 (Eq. 9) correlates well with both experimental traces.

Table 1 lists the peak current heights corresponding to each of the experimental methods and simulations over a range of pulse amplitudes. In the case of the differential pulse waveform the correlation between experimental peak current heights and those predicted by Model 2 occurs only over a narrow pulse amplitude range. However it can be seen that the peak current heights obtained by numerically differentiating the sigmoidal experimental plot correlate well with those predicted by Model 2 over the complete range of pulse amplitudes studied. It is therefore possible to enjoy the advantage of a peaked response which is well-defined (Model 2) over a wide range of pulse amplitudes without having to invest in new and sophisticated equipment, the only system requirements being a linear ramp waveform generator, a data acquisition unit and a computer with relevant software, all of which are commonplace in any electrochemistry laboratory.

The results for peak current from Model 2 and peak current values from the numerical derivative of a linear sweep correlate well. The reason for slight differences may be because of the fast sweep rate used (10 mV/s). However the experimental differential pulse response deviates from Model 2, indicating that there may be some contribution to the response from the pulse and that a steady state has not occurred in the timescale of the pulse width. This may be due to slow electron transfer kinetics on such a short time scale or a combination of slow electron transfer kinetics and diffusion control.

As stated earlier Model 2 is based on the fact that a steady-state current is reached within the pulse width due to the presence of edge effects which in turn are due to the thickness of the diffusion layer being of the same order of magnitude as the electrode diameter. The diffusion layer thickness (d) is approximated by the equation $d = (\pi Dt)^{1/2} = 1.06 \times 10^{-5}$ m where t = pulse width = 55 ms. Therefore the thickness of the diffusion layer (d) is controlled by the pulse width (t), and the diffusion coefficient (D), both of which are constant for a given set of experimental conditions. It is clear that the extent to which Model 2 can be applied to a given experimental arrangement depends directly on the relative magnitudes of the electrode diameter and the diffusion layer thickness.

A distinct advantage of applying a differential pulse to a microelectrode can be seen at lower concentrations. This is evident in Figure 3 where the response is shown both for direct current and the differential current following the application of a differential pulse. The direct current response is very difficult to interpret and therefore almost useless in providing analytical information. However for the differential pulse response there is useful information to be gained as a peak is clearly seen at the potential at which the electrochemical reaction in question is known to occur. This has the effect of lowering the limits of detection relative to the direct current experiments. Also a peaked response is more desirable as a baseline can be drawn enabling peak current to be easily

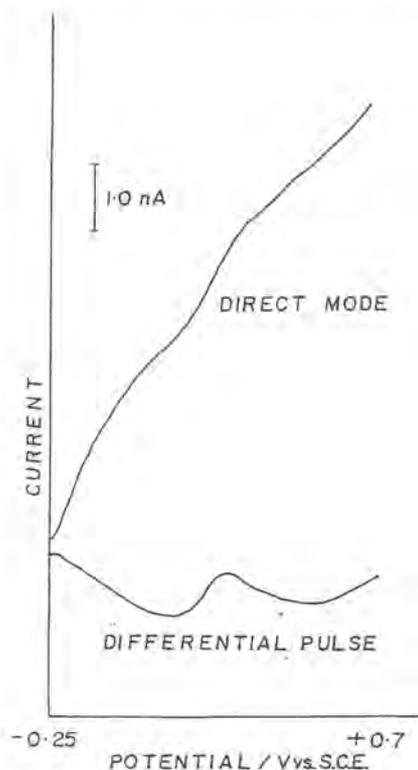


Fig. 3. Comparison of the responses produced by the application of a linear sweep and a differential pulse waveform at a microelectrode in a solution of 5 mM $[\text{Fe}(\text{CN})_6]^{4-}$ in 0.1 M KCl. Platinum microelectrode of radius 4.46×10^{-6} m, scan rate in both cases was 10 mV s^{-1} and in the case of the differential pulse the time constant: 1.0 s, differential pulse waveform period: 1.0 s, pulse width = 55×10^{-3} s and the pulse amplitude: 100 mV.

determined. This is in stark contrast to the difficulties encountered when attempting to measure limiting current from a direct current microelectrode experiment at submillimolar concentrations.

In conclusion, there is good correlation between Model 2 and the numerical derivative of a linear sweep potential waveform applied to a microelectrode. A differential pulse study does not correlate as well perhaps due to slow kinetics. Model 1 will apply for larger electrodes. Work on examining the effect of slow kinetics on the response is ongoing.

Experimental

The potentiostat used throughout this work was an Edr Model ECP 100 and a J.J. Lloyd X-Y chart recorder Model PL3 was used to chart the response. A three electrode system consisting of a carbon rod auxiliary, a saturated calomel reference electrode and an EG&G Parc platinum planar disk microelectrode was employed. All chemicals used were of reagent grade and all solutions were made up using deionized water. Solutions were degassed by bubbling with nitrogen for at least 15 min prior to recording any data. A Pasco Scientific CI-6510 analogue to digital converter was used to collect and store the data digitally and the simulations were carried out using a program written in Microsoft Excel.

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